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Review Article

Phototherapy — a treatment modality for wound healing and pain relief

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ABSTRACT

When applied properly, phototherapy or Low Level Laser Therapy (LLLT) has proved to be very efficient in relieving pain and improving wound healing. However, until recently there has been a lack of scientific scrutiny concerning the clinical efficacy of this procedure. This does not mean that phototherapy does not work. A search for “laser” and “therapy” on the ISI Web of Knowledge database reported that the USA accounts for 35.69% of the research material while only 18 papers were reported from South Africa (1987-2006) which accounts for 0.17% of the 10 652 papers analyzed. Despite the lack of scientific research, clinical results have been exceptional. Clinicians around the world, based on their professional experiences, confirm the analgesic effect of phototherapy. Unfortunately, from a strictly scientific point of view, these reports are hardly conclusive. There has been little or no standardization in the application of phototherapy. This review investigates key aspects of phototherapy and the efficacy of laser therapy for specific applications namely, wound healing and pain relief.

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Keywords: wound healing, pain relief, LLLT, phototherapy, laser

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INTRODUCTION

The use of laser as a non-surgical medical treatment modality for assisting the normal processes of healing has increased over the last few years. However, the efficacy of laser in reducing pain or promoting tissue repair still remains controversial (Enwemeka *et al*, 2004). Laser therapy aims to restore the normal biological function of injured or stressed cells so 'Normalization' is the keystone of laser therapy (Tunér and Hode, 2002). The stimulatory effect of laser therapy can be seen in wounded cells or in cells that are growing sub-optimally whereas cells that are normal or fully functional remain unaffected and no therapeutic effect can be observed (Smith, 1991).

1. Photobiology

Laser light has the unique properties of monochromaticity (a single wavelength), collimation (travels in a single direction without divergence) and coherence (with all waves in phase) (Matic *et al*, 2003). These properties are what allows laser light to penetrate the skin surface non-invasively (Matic *et al*, 2003; Theralase, 2003; Schindl *et al.*, 1999). Therapeutic lasers are athermic with no appreciable heat transfer (<0.65 °C) so the photonic energy is transferred directly to the target cells and thermal damage is avoided (Matic *et al*, 2003; Theralase, 2003). Therapeutic lasers use monochromatic light in the 630 to 905 nm range, known as the "therapeutic window" (Stadler *et al*, 2004).

Cellular effects of phototherapy can be classified into primary (light-induced), secondary (which occur in response to the primary effects) and tertiary effects (Schindl *et al*, 1999; Stadler *et al*, 2004; Dyson, 2006). Primary reactions are generally restricted to the absorption of photons while secondary effects are not unique to phototherapy and, because their occurrence depends on the sensitivity of the cells, are less predictable than primary effects (Dyson, 2006). Tertiary effects are the least predictable since the response is influenced by the internal and external environment and by intracellular interactions. The tertiary effect is also known as the systemic effect and explains why the treatment of one lesion can stimulate the healing of both the directly treated lesion and other lesions that

the patient may have (Dyson, 2006).

In primary responses, photons emitted by the laser reach the mitochondria (Theralase, 2003) and cell membranes of low lying cells (fibroblasts, keratinocytes or endothelial) where the photonic energy is absorbed (Olsen *et al.*, 1980) by chromophores (mitochondrial cytochromes, porphyrins and flavoproteins) and is converted to chemical kinetic energy (Matic *et al*, 2003) within the cell. This causes changes in membrane permeability, improved signaling between mitochondria, nucleus and cytosol, nitric oxide formation and increased oxidative metabolism to produce more ATP (Morimoto *et al*, 1994; Yu *et al*, 1997; Karu, 1989), which ultimately leads to normalization of cell function, pain relief and wound healing (Figure 1) (Matic *et al*, 2003; Dyson, 2006; Olsen *et al*, 1980).

Secondary reactions lead to the amplification of the above-mentioned primary photoreactions. A cascade of metabolic effects results in various physiological changes at the cellular level such as changes in cell membrane permeability (Figure 1) (Smith, 1991; Dyson, 2006; Olsen *et al*, 1980). Calcium is released from the mitochondria into the cytoplasm with changes in intracellular calcium levels (Tunér and Hode, 2002; Smith, 1991) which stimulates cell metabolism and the regulation of signaling pathways responsible for significant events required for wound repair such as cell migration, RNA and DNA synthesis, cell mitosis, protein secretion and cell proliferation (Takac and Stojanovic, 1998; Klepeis *et al*, 2001).

Tertiary effects are induced in cells at a distance from the cells in which the secondary events occur (Dyson, 2006). Irradiated or energized cells communicate with each other, and with non-irradiated cells, through increased levels of cytokines or growth factors (Smith, 1991; Vladimirov, 2004) resulting in inter-cellular communication (Tunér and Hode, 2002). There is an increase in the immune response with the activation of T-lymphocytes, macrophages and number of mast cells (Hamblin and Deidova, 2006). An increase in the synthesis of endorphins and decrease in bradykinin results in pain relief.

Studies have matched action spectra for biostimulation with absorption spectra of

cytochrome c oxidase and have found remarkable similarities in the red and near-infrared (IR) regions of the spectrum (Hamblin and Deidova, 2006). All the individual oxidation states of the cytochrome c oxidase enzyme have different absorption spectra, thus probably accounting for differences in the action spectra of LLLT. The wavelength range important for phototherapy (600-860 nm) has four active regions, but peak positions are not exactly the

same for all action spectra. The peak positions are between 613.5 and 623.5 nm (in one spectrum, at 606 nm) in the red maximum. The far-red maximum has exact peak positions between 667.5 and 683.7 nm while two near-infrared maxima have peak positions in the range 750.7-772.3 nm and 812.5-846.0 nm, respectively (Karu and Kolyakov, 2005).

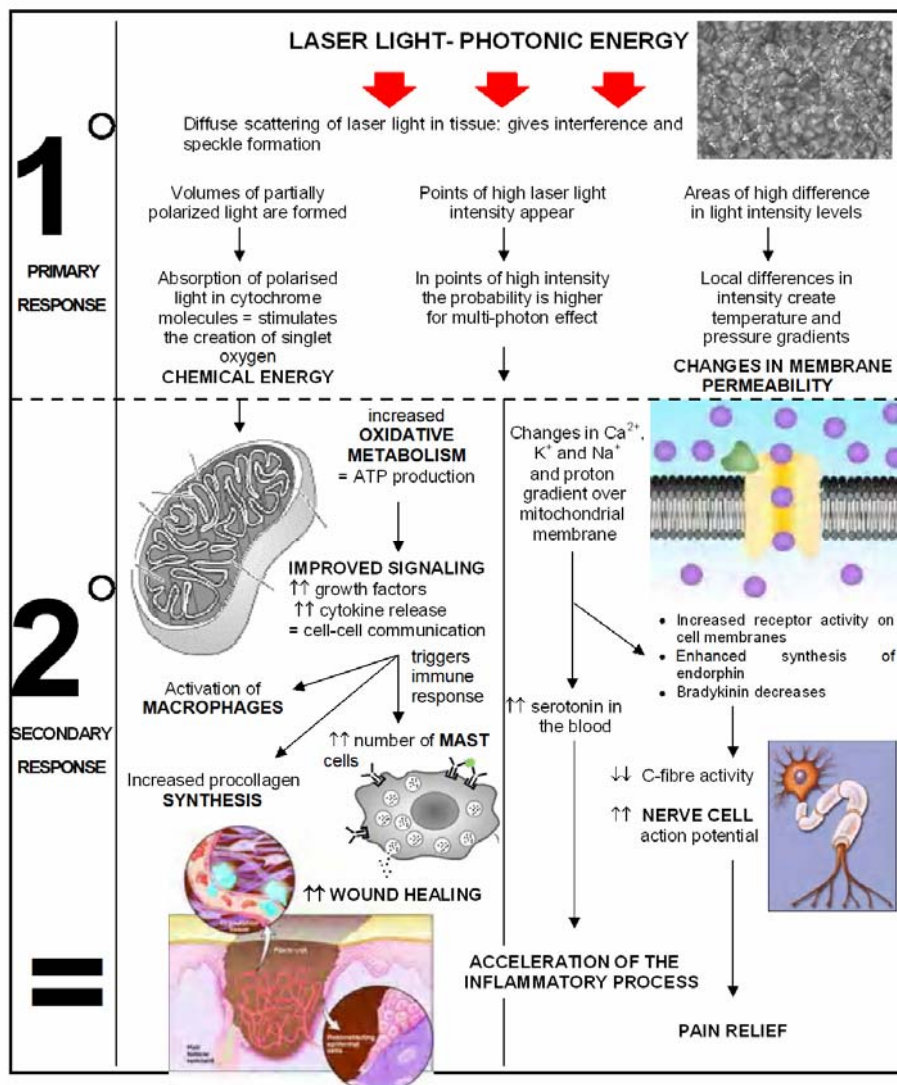


Figure 1.

The primary mechanisms relate to the interaction between photons and molecules in tissue, while the secondary mechanisms relate to the effect of the chemical changes induced by the primary effects. The stimulation of cellular ATP production has been suggested as one of the most important effects of laser therapy. The secondary mechanisms include effect on pain, effect on blood circulation, effect on stimulatory and regulatory mechanisms and effects on the immune system. Adapted and modified from the original text of Tunér and Hode (2002).

Other mechanisms may be operating in LLLT. Certain molecules such as porphyrins can be converted into a long-lived triplet state after photon absorption. This triplet state can interact with ground-state oxygen with energy transfer leading to the production of a reactive singlet oxygen species (Hamblin and Deidova, 2006). Another proposed mechanism is the alteration of mitochondrial

metabolism and activation of the respiratory chain by illumination, which would also increase production of superoxide anions O_2^- . It has also been proposed that laser irradiation could reverse the inhibition of cytochrome c oxidase by nitric oxide (NO) and thus increase the rate of respiration with consequently more ATP synthesis (Hamblin and Deidova, 2006).



	MINIMUM TREATMENT	MAXIMUM TREATMENT
Dose or energy density		
	Superficial wounds	Musculoskeletal pain
	Open wound HeNe, 632.8 nm 630 nm-700 nm diode 904 nm GaAs Wound periphery HeNe, 632.8 nm 630 nm-700 nm diode 904 nm GaAs	Chronic wound HeNe, 632.8 nm Wound periphery HeNe, 632.8 nm
	Superficial pain HeNe, 632.8 nm 630 nm-700nm diode 904 nm GaAs	Deep lying pain 904 nm GaAs 870 nm GaAIAs
Continuous vs pulsed	HeNe 632.8 nm – continuous GaAs 904 nm - pulsed Pulsed: use average output power to calculate dose	GaAIAs 780,820,870 nm – continuous CW: use output power to calculate dose
Wavelength of probe	Superficial wound, < penetration, visible light probe (632.8 nm, 660 nm)	Deep wound, > penetration, musculoskeletal injury, infrared probe (904 nm)
Contact vs non-contact	1-2 cm from the wound and the periphery of the wound is treated in skin contact. For superficial problems the probe is held in light contact with the skin	For medium or deep problems the probe is held with pressure in direct contact with the skin to increase the penetration depth.
Pigmentation	Light complexion – better penetration	Dark complexion – absorbs the light and reduces penetration
Treatment area	Muscle, bone, ligament – better penetration	Adipose or highly vascular tissue – reduces penetration. Deeper tissues require more treatment
Treatment interval	Acute wounds or musculoskeletal injury – daily Every third day for 2 weeks then once a week for a few weeks.	Chronic wounds or injury – 1 or 2 weekly Infected ulcers – twice weekly until infection clears

Figure 2.

Key aspects of phototherapy that can be used to establish an effective therapeutic regimen for the treatment of superficial wounds or skin conditions and musculoskeletal injuries.

Key aspects that influence phototherapy can be used as guide to establish an effective therapeutic regimen for the treatment of superficial wounds or skin conditions and musculoskeletal injuries (Figure 2). Some of the key aspects include:

Lasers: Diode lasers emit light with a shorter coherence length than Helium-Neon (HeNe, 632.8nm) lasers and the biological effects of light from a 633 nm diode laser are less obvious than those from a HeNe laser. A diode laser can obtain similar results by using a higher power output (25-50 mW) and higher doses (Tunér and Hode, 2002; Ohshiro and Calderhead, 1988).

Wavelength: Wavelength is the distance between two peaks of a wave. The symbol for wavelength is λ (lambda) and the unit of measurement is nanometers (nm) (Peavy, 2002). The penetration of laser light depends on the wavelength, the output power and the treatment technique used. (Tunér and Hode, 2002; Theralase, 2003; Pontinen, 1992).

Power: The unit of power is Watt (W) and since the laser output power is low it is expressed in milliwatts (mW) (Peavy, 2002). The power density or light intensity of the beam on the tissue surface is expressed in mW/cm^2 which is the power divided by the area of the target tissue being illuminated by the laser light (Schindl *et al*, 1999; van Breugal and Dop Bar, 1992). The stronger the power output (mW) the shorter the treatment time.

Energy density: (dose or fluence) is expressed in Joules per cm^2 (J/cm^2), which is the product of power (mW) and time (s) per spot size (cm^2) (Tunér and Hode, 2002; Ohshiro and Calderhead, 1988). The dose administered is influenced by the power, time, irradiance (power density) and treatment intervals but the dose required depends on the wavelength, type of tissue, condition and depth of target tissue, chronic or acute problem, pigmentation and treatment technique (contact versus non-contact) (van Breugal and Dop Bar, 1992; Woodruff *et al*, 2004; Baxter *et al*, 1997). Biostimulatory studies report using doses from as low as $0.001 \text{ J}/\text{cm}^2$ to $10 \text{ J}/\text{cm}^2$ however effective doses of near-IR light may be much higher than $10 \text{ J}/\text{cm}^2$ especially for deep lesions. Doses that are too low result in a weak effect with no observable effect. If a dose above the highest one suitable is administered (van Breugal

and Dop Bar, 1992), a negative or minimal effect is detected. With an even greater dose, a bio-suppressive or inhibitory effect may be observed (Coombe *et al*, 2001). In treatment, the dose is often referred to as the number of Joules per point where a point is defined as an area that is 5 mm in diameter (0.2 cm^2) or less.

Continuous versus pulsed wave technology: A light source that emits light at a constant intensity is known as continuous wave (CW) emission whereas pulsed light has varying intensity (Ohshiro and Calderhead, 1988). When a laser is pulsed, the laser light power varies between the pulse peak output power and zero so the average power is used to calculate the dose while continuous wave lasers use the output power (mW).

Contact versus non-contact: A laser can be used in a scanning mode or in contact with the surface of the skin, with or without pressure and held flat against the skin or with the aperture protruding (Ohshiro and Calderhead, 1988; Pontinen, 1992). In order for a laser system to provide optimal penetration through the skin it must be in direct contact with the skin and at an incident angle of 90 degrees (perpendicular to the skin) (Ohshiro and Calderhead, 1988; Mendez *et al*, 2004). This will minimize any reflection from the skin's surface and allow the best penetration into the tissue.

2. Therapeutic applications

Several studies have demonstrated either a stimulatory or inhibitory effect of phototherapy on healing mechanisms using *in vitro* cell culture studies (van Breugal and Dop Bar, 1992). *In vivo* studies have demonstrated that phototherapy has a positive effect on wound healing in the clinical environment; however the exact mechanism is still not completely understood since a specific therapeutic window, dosimetry or mechanism of action has not been determined (Smith, 1991; Coombe *et al*, 2001; Karu *et al*, 1984). The effect on the patient and how it effects healing has however been well documented but the lack of knowledge complicates the evaluation of conflicting reports found in literature (Tunér and Hode, 2002). Lack of quality control has produced negative results in some studies and criticism of many of the positive

studies (Tunér and Hode, 2002). Studies claim that laser therapy dramatically reduces healing time compared to other traditionally used modalities. Hospitals in the UK use laser therapy in post-surgical recovery rooms and have found that patients have less pain, take 50% less pain medication, heal in half the time and have significantly less scar tissue (Rudnick, 2005). However, Allendorf *et al*, (1997) reported that HeNe laser irradiation ($1\text{J}/\text{cm}^2$, $2\text{J}/\text{cm}^2$ and $4\text{J}/\text{cm}^2$) had no measurable benefit on wound healing and a biostimulatory mechanism could not be elucidated. Likewise, Colver and Priestley (1989) concluded that HeNe (633 nm, 5 mW, 1 mm diameter beam) laser irradiation (three times a day for 3 days) did not have any significant effect on cell proliferation.

Trelles *et al*, (1989) reviewed the use of local irradiation with phototherapy and found this approach elicited the following types of effects: biostimulatory, analgesic, anti-exudative, anti-haemorrhagic, anti-inflammatory, anti-neuralgic, anti-oedematous, anti-spasmodic and vasodilatory. Furthermore, Medrado *et al*, (2003) studied the effect of LLLT on wound healing and concluded laser therapy reduced the inflammatory reaction and increased collagen deposition with a greater proliferation of myofibroblasts in experimental cutaneous wounds. Both studies found the main clinical uses of LLLT included wound healing, pain control, soft tissue injury, arthropathy, osteopathy and treatment of existing scars (Medrado *et al*, 2003; Trelles *et al*, 1989).

Some of the clinical effects of phototherapy are that it:

1. reduces pain in a large variety of acute and chronic pain entities including pain related to abnormalities in nerves, soft tissue, muscles, tendons, joints and bone.
2. reduces swelling and inflammation associated with acute injuries in superficial muscles, tendons, ligaments, bursae, and sheaths (Smith, 1991; Woodruff *et al*, 2004; de Freitas *et al*, 2001),
3. improves wound healing of slow-to-heal or non-healing wounds in soft tissues, tendons and bone due to improved tissue oxygenation and nutrition (Takac and Stojanovic, 1998; Woodruff *et al*, 2004; Kubota, 2004; Gabel,

1995),

4. improves absorption of interstitial fluid (anti-oedematous) and increases lymphatic circulation and drainage which results in better tissue regeneration (Takac and Stojanovic, 1998),
5. improves local and systemic blood circulation which is useful in blood-related conditions such as Buerger's and Raynaud's diseases and torpid leg ulcers,
6. enhance autoimmune response in immune-deficient conditions such as psoriasis, rheumatoid arthritis and atopic dermatitis (Woodruff *et al*, 2004),
7. controls hypertension by increasing flow rate and increasing the diameter of the vessel (Gabel, 1995), and
8. restores normal pigment in abnormally coloured cutaneous lesions.

Laser therapy also has benefits for patients with Bell's palsy, psoriasis and unhealed donor areas following skin grafting (Baxter *et al*, 1997). A neodymium:yttrium-aluminum garnet (Nd:YAG, 1064 nm) laser with the correct dosage, as with other lasers, can be used to successfully treat herpes simplex lesions (Ohshiro and Calderhead, 1988).

3. Phototherapy for superficial wound healing

The types of wounds that can be mentioned under wound healing not only include pressure sores and ulcers, but also burns, skin donor areas and post-operative wounds (Ohshiro and Calderhead, 1988; Pontinen, 1992; Baxter *et al*, 1997). Franks and Gilbert (1998) reported rapid demarcation of chronic wounds after initial treatment with clearance of necrotic or sloughy tissue, reduced signs of infection, reduced amount and odour of fluid in highly exuding wounds, reduced pain and resumption of the immune response initiated by the inflammatory phase.

Medrado *et al*, (2003) evaluated the effects of laser therapy in experimental cutaneous wound healing and concluded that a dose of $4\text{J}/\text{cm}^2$ was superior to that of $8\text{J}/\text{cm}^2$. Furthermore, Hawkins and Abrahamse (2005b; 2006a) reported that $5\text{J}/\text{cm}^2$ using a HeNe laser stimulates mitochondrial activity, which leads to normalization of cell function and ultimately stimulates cell proliferation and migration of wounded fibroblasts to accelerate wound closure

while a dose of 10 J/cm^2 was associated with a significant amount of cellular and molecular damage. Pereira *et al*, (2002) studied the effect of a 120 mW GaAs diode laser on fibroblasts and concluded that 3 J/cm^2 stimulated fibroblast proliferation without impairing procollagen synthesis. Pourzarandian *et al*, (2005) studied the effect of Er:YAG laser irradiation on cell growth of cultured human gingival fibroblasts and concluded that the optimal stimulative energy density was 3.37 J/cm^2 . The results indicate that Er:YAG laser irradiation may benefit wound healing.

A visible light probe (630-780 nm) has a penetration depth of a few millimetres (0.5-50 mm) and is used for wound healing and superficial skin conditions (Olsen *et al*, 1980; Moore *et al*, 2002). Of four different wavelengths tested (660 nm, 820 nm, 880 nm and 950 nm), Karu *et al*, (1993) found that 660 nm was the most effective. A 660 nm probe followed by a cluster of five 660 nm diodes is usually recommended for superficial wounds and skin conditions (van Breugal and Dop Bar, 1992). For acne, scar tissue and small lesions a visible red (660 nm) single point laser probe (30 mW) is usually recommended. Large cluster probes are usually used for large wounds or burns where the treatment area requires a deeper effect with a reduced treatment time. For wounds at a medium depth the probe is pressed against the skin. The deeper the tissue to be treated the higher the pressure. For open wounds or ulcers, the laser probe is normally held 1-2cm from the wound while the periphery is treated with the laser probe in direct contact. The open area of the wound should receive a lower dose than the skin periphery (Tunér and Hode, 2002). A single laser probe (660 nm) can be used around the wound margin of superficial wounds while a cluster probe (visible red and infra-red laser light) can be used for the soft tissue inflammation. In the treatment of a chronic ulcer for example, a higher dose such as 3-4 J/cm^2 will be used on points along the periphery of the wound followed by a lower dose of 0.5 J/cm^2 over the open wound (Tunér and Hode, 2002; Ohshiro and Calderhead, 1988). The open wound needs a lower dosage than the skin-covered periphery as the laser light is not reflected or scattered but rather absorbed by the skin in the unprotected wound since it hits the uncovered cells

directly.

There remains some controversy over whether infected wounds do indeed respond better to laser treatment so special precautions such as holding the probe close (non-contact) to the wound and cleaning the probe with an alcohol wipe have to be used to reduce contamination during laser treatment (Tunér and Hode, 2002; Ohshiro and Calderhead, 1988; Baxter *et al*, 1997). Nussbaum *et al*, (2002; 2003) reported that phototherapy using a wavelength of 630 nm ($1-20 \text{ J/cm}^2$) results in bacterial inhibition which may be an important consideration when selecting the correct wavelength for infected wounds (Lucas *et al*, 2003). An infected ulcer can be treated twice weekly until the infection clears. Patients on prescribed medication or who have conditions known to cause photosensitivity reactions should also avoid LLLT. It is unlikely that a combination of laser and drug will trigger a photosensitivity response however patients should be patch tested with a small dose and examined after 24-48 hours to determine if there is a hypersensitivity reaction.

Acute wounds should be treated daily while chronic wounds should be treated 1-2 times a week (Ohshiro and Calderhead, 1988). When treating through a dark complexion, adipose or highly vascular tissue, more light will be absorbed with reduced penetration to the target tissue, so a greater irradiance will be required in order to achieve the same biological effect (Stadler *et al*, 2004; Greppi, 2001). Chronic tissue conditions require more treatment intervals where two or three treatments a week are considered as the maximum (Ohshiro and Calderhead, 1988). The deeper the lesion or target tissue the more treatment will be required. It has been shown to be beneficial to treat at closer intervals in the beginning (every other day or every third day for two weeks) and then at longer intervals (once a week for several weeks). As a general rule, it is better to use 3-4 treatments a week with moderate doses than using higher doses and fewer treatments (Tunér and Hode, 2002).

4. Phototherapy for musculoskeletal pain relief

Soft tissue injuries such as tendonopathies (tendonitis and tenosynovitis) and ligamentous injuries are easier to treat since the lesions are easier to locate and palpate (Ohshiro and Calderhead,

1988; Woodruff *et al*, 2004). Various arthritic conditions have been identified as responding well to laser therapy particularly where osteoarthritis has affected the small joints of the hands and feet (Ohshiro and Calderhead, 1988). Laser therapy provides relief for musculoskeletal pain, post-fracture pain, pain at origin or insertion of any muscle or tendon, haematoma, and neurogenic pain (Ohshiro and Calderhead, 1988). Most acute musculoskeletal injuries should be treated daily over a short period whereas chronic musculoskeletal injuries should be treated over a longer period every week if palliative or every 2-3 days if there is low grade inflammation (Tunér and Hode, 2002). Laser therapy has also been indicated for other painful conditions such as shingles (Ohshiro and Calderhead, 1988). Moore *et al*, (2002) concluded that there was a 50% reduction in the severity of pain and 50% reduction in the use of analgesics in patients receiving 24 J/cm² per point when compared to the control group. Gaida *et al*, (2004) showed that 670 nm laser irradiation of burn scars using 400 mW twice a week over 8 weeks had a positive effect on the macroscopic appearance, pruritus and pain.

An infra-red probe has a penetration depth of several centimetres and is used for musculoskeletal injuries, acupoints, neurogenic pain and trigger points (Theralase, 2003; Moore *et al*, 2002). The most frequently used laser for pain therapy is the GaAlAs diode that emits coherent light in the near-infrared waveband, usually 820-840 nm, and with a continuous wave power output of 60 mW (Moore *et al*, 2002). A near infrared (810 nm) laser probe can be used to treat pain while a cluster probe can be used for soft tissue inflammation and pain trigger points (muscle, tendon and ligaments). The greatest active depth is achieved when the laser probe is held in direct contact with the skin and the probe is pressed against the skin.

5. Current and future directions

In vitro studies currently being performed by the Laser Research Group include investigating the effect of 632.8 nm HeNe, 830 nm diode and 1064 nm Nd:YAG laser irradiation on normal, wounded, diabetic and diabetic wounded fibroblast cells. (Hawkins and Abrahamse, 2005a; 2005b; 2006a; 2006b; 2007a; 2007b). The *in vitro* studies have

established important laser variables such as dose (J/cm²) (Hawkins and Abrahamse, 2005b, 2006a), number of exposures (Hawkins and Abrahamse, 2006b) and specific irradiation conditions (Hawkins and Abrahamse, 2007a) that accelerate wound closure, cell-cell communication and cell proliferation and these *in vitro* results may be used as a guideline for the initiation of a clinical study. Future studies include investigating other conditions of cell stress or damage such as a change in intracellular pH to mimic metabolic acidosis that is common with diabetes, a reduction in the oxygen tension (pO₂) or hypoxia that is common in chronic inflammation and indolent wounds (Yu *et al*, 2002) and *in vitro* ischemia that is common in ischemic heart disease, stroke and hypoxia (Abercrombie, 1966). The results from these *in vitro* studies will be used to investigate the effect of laser irradiation on a wounded three-dimensional (3D) artificial skin construct. The skin equivalent is a suitable alternative method to animal testing since it represents an advanced alternative to normal cell culture and its natural 3D structure closely reproduces an *in vivo* situation. In addition, the potential use of laser irradiation on the stimulation of adult adipose derived stem cell differentiation for the use as autologous grafts in wound healing is being investigated.

Conclusion

Lasers are widely used for pain relief and wound healing without negative or long-term side effects (Theralase, 2003; Coombe *et al*, 2001). Laser therapy allows the user to combine different probes or cluster heads depending on the laser that is available and the specific application. For example, a 660 nm probe can be used to treat the periphery of a superficial wound followed by a cluster probe of visible and infrared laser light for the soft tissue and inflammation. The laser treatment parameters can be changed and adapted depending on the type of laser used (visible or infra-red, continuous or pulsed) and the application (acute or chronic). The most important parameter that should be maintained is the dose or the energy density (J/cm²). Factors such as contact or non-contact method and the treatment interval can be modified and adapted according to the specific application and treatment area.

In order to monitor the effects of the therapy, a record should be kept that includes a comprehensive list of the treatment parameters and documents changes or any signs of improvement (Pontinen, 1992). Laser therapy requires the user to test and re-test after the laser therapy to determine if there are any signs of improvement in terms of movement, pain relief or wound healing. Since laser has a systemic effect, it is important to observe caution in interpreting results of studies in which laser has treated one part of the body while another part of the same body has been used as a control (Tunér and Hode, 2002). Some patients require a combination of medications and will respond to LLLT used in combination with other therapeutic modalities. If no improvement is noted after several treatments the therapy should be discontinued. Laser users have reported a good success rate for a wide range of applications in veterinary, health, dentistry (Pourzarandian *et al*, 2005) and physiotherapy for both wound healing and pain relief. Enwemeka *et al*, (2004) conducted a meta-analysis on 34 peer-reviewed papers and concluded that laser phototherapy is a highly effective therapeutic armamentarium for tissue repair and pain relief. By improving the study design as well as the reporting of all the variables used in trials, laser therapy may become as well recognized as laser surgery. In order to obtain full acceptance as a valid medical modality, new and high quality studies are required (Tunér and Hode, 2002).

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